COMPUTATIONAL CELL BIOMECHANICS

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Aim

Tumour is nowadays one the most concerning worldwide disease that causes millions of deaths each year. Furthermore, the intrinsic inter and intra tumour variability make it difficult to investigate the mechanical properties of cancerous cells. The aim of the research activity is the development of a computational model of the cell biomechanics. The use of Finite Element Models (FEMs) would provide major advantageous capabilities such as: (i) observing the mechanical contributions of the cell subcomponents, (ii) controlling the variables involved in the overall response and (iii) providing reproducibility to the mechanical results.

Materials and Methods

The virtual solid model has been realized with the FE software Abaqus CAE 2019 (Dassault Systèmes Simulia Corp., Providence, RI).

FE model of the cell

The cell is a complex biological structure, for this reason the model has been reduced to its main subcomponents (fig. 1):

- Cytoplasm
- Plasma membrane

Continuum-tensegrity structure

Both continuous and discrete structures have been used to describe the subcomponents. In particular, the cytoskeleton was modelled by means of a network of truss elements, building a tensegrity structure that provides a prestress to the overall structure.

Material Formulation

Viscohyperelastic material properties were assigned to each subcomponents using a Neo-Hookean formulation. Special attention was given to the cytoplasm and to the cytoskeleton. Prestress was described by means of thermal expansion and predefined fields.



Fig.1: Finite Element Model of the cell with its subcomponents: (a) cytoplasm, (b) plasma membrane, (c) cytoskeleton and (d) nucleus.



- > Nucleus
- Cytoskeleton

The model has been discretized by means of linear hexahedral elements and truss elements (fig. 2).

Results

Strain hardening due to prestress.

- Strain hardening is a phenomenon observed in cells due to the tensegrity structure of the cytoskeleton [1].
- Most of the stress is concentred along the cytoskeleton trusses. This highlights the role of the cytoskeleton in the cell mechanical response.
- Applying a thermal expansion (to simulate prestress) to the cytoskeleton, causes a non linear increase in the cell stiffness (fig. 3).



$$\varepsilon^{th} = \alpha \big(\vartheta, f_{\beta}\big)(\theta - 0^{0}) - \alpha \big(\theta^{I}, f_{\beta}^{I}\big)(\vartheta^{I} - \theta^{0})$$

Fig.2: Finite Element Finite element discretization of the cell and its subcomponents.

Simulation of experimental setups

- The cell model provided good fit to the usual mechanical experimental setups used to assess the cell biomechanics.
- Both Atomic Force Microscopy indentation technique (fig. 4) and micropipette aspiration (fig. 5) were used to validate and test the model [2,3].



Fig. 4: Simulations of the AFM indentation experiments to observe the behaviour of the continuous model against the continuous-tensegrity model.

Micropipette aspiration tests



Fig. 3: Effects of the prestress on the mechanical response of the cell. (a) and (b), distribution of the stresses along the truss elements of the cytoskeleton. (b) Schematics of the forces applied to the cell during the simulation. (d) non-linear increase of the cell stiffness due to the prestress.

Discussion

- The differences between the homogeneous and the continuumtensegrity models were assessed when referring to cell subcomponents.
- \succ The model can mimic the behaviour of an average human cell.
- Role of prestress: structural stability to the cell.
- Cytoskeleton: tensile behaviour, Cytoplasm: compression behaviour.
- > Different ratios of cell and pipette (D_c/D_p) diameters strongly influence the global response of the cell during MPA.

FE models can be applied to deepen the knowledge about cell biomechanics.

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Fig. 5: Simulations of the micropipette aspiration experiments to analyze the effect of varying the ratio between the micropipette radius and the cell radius.

References

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